

The impact of processing workflow in performance of automatic white matter lesion segmentation in Multiple Sclerosis

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The logo for VisAGeS is located in the top-left corner. It features a stylized white dome or canopy structure with a grid of lines, set against a dark blue background. Below the dome, the text "VisAGeS" is written in a bold, orange, sans-serif font.

Summary

- Introduction
- STREMe1
- STREMe2
- Workflow
 - Intensity inhomogeneity correction
 - Denoising
- Results
- Conclusions

Introduction

- There is many algorithms for MS lesion segmentation
 - Little information available about the preprocessing algorithms employed
- Evaluate the need of denoising and intensity inhomogeneity correction

- Method introduced by (Ait-Ali et Al., MICCAI 2005)
- Model-based segmentation
 - Lesions are considered outliers to the model
- Three steps:
 1. Robust estimation of NABT parameters
 2. Refinement of outliers detection
 3. Application of lesion rules

- 3-class Finite Multivariate Gaussian Mixture Model
- Modified Expectation-Maximization algorithm (mEM)
 - Trimmed Likelihood (Neikov et al. 2006)

$$TL = \sum_{i=1}^{n-h} f(x_{\nu(i)}; \Theta)$$

- Ordering function

$$f(x_{\nu(1)}; \Theta) \geq f(x_{\nu(2)}; \Theta) \geq \dots \geq f(x_{\nu(n)}; \Theta)$$

- In our experiments $h=n/10$

Outliers detection

- mEM gives a fixed number of outliers (h)
- h can contain voxels that fit the NABT model
- Compute Mahalanobis distance:

$$d_{i,j} = (\mathbf{y}_i - \mu_j)^T \Sigma_j^{-1} (\mathbf{y}_i - \mu_j)$$

- Mahalanobis distance follow a χ^2 law with m d.o.f
 - m is the number of sequences
 - A threshold is defined by the χ^2 law for a given p-value

Application of lesion rules

- Outliers have different sources:
 - Lesions
 - Registration errors, vessels, noise, etc.
- Rules to select lesions

(compared to WM)	T1-w	T2-w	PD-w	FLAIR
T2-w lesions	Isointensity or Hypointensity	Hyperintensity	Hyperintensity	Hyperintensity

- STREMv1
 - Atlas registration for initialization:
 - Time consuming
 - Problems with tissue atrophy in samples with huge lesion loads
 - Segmentation only based on MR intensity
- STREMv1.5
 - Improve initialization of mEM
- STREMv2
 - STREMv1.5 + Reduction of false positives

Initialization of mEM

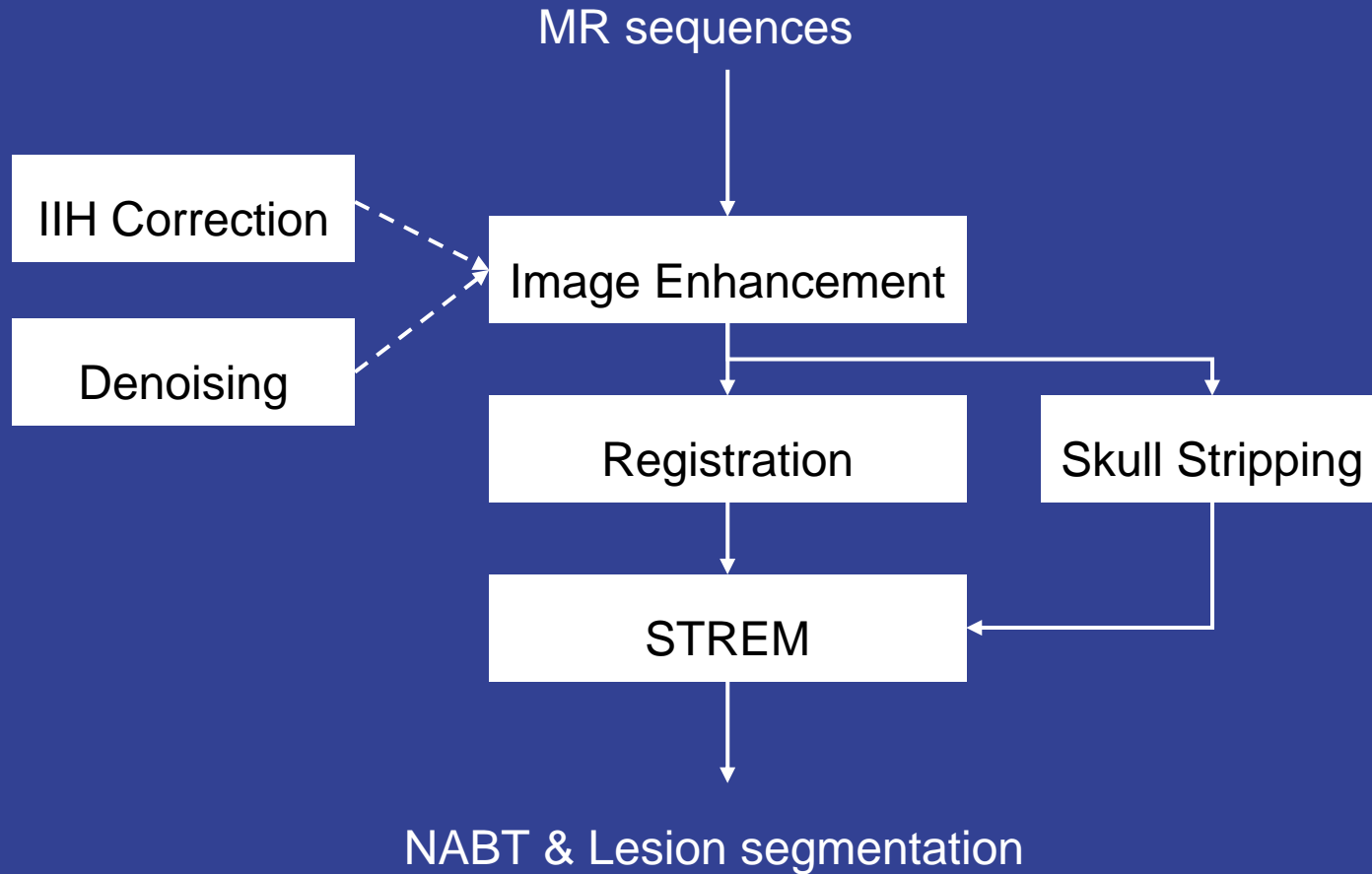
- Multiple random initializations
 - Computationally time expensive
 - No guarantee for global convergence
 - No general agreement on how many initializations are necessary, but they are growing with the number of dimensions

Initialization of mEM

- Hierarchical multiple initializations on T1-w only:
 1. n_0 random initializations
 2. Use mEM with $iter_0$ iterations using these initializations
 3. Keep n_1 best solutions
 4. Use mEM with n_1 partial solutions until convergence
 5. Keep best solution
 - $n_0=300$, $iter_0=10$ and $n_1=10$
- Expansion to multidimensional mEM
 - Probabilities at the end of E-step in T1-w are applied in the multidimensional M-Step

Spatial Constraints

- Detection of false positives:
 - Isolated hyperintensity voxels due to image noise are misclassified
 - In the cortex and CSF, voxels can have the same MR intensity as WML
- Two rules are added:
 - Minimal size of WM lesion is defined as 3mm^3
 - MS lesions have to be contiguous to white matter



- Skullstripping
 - Use BET (Smith 2002)
 - Manually corrected
- Rigid registration
 - Use Mutual Information with NEWUOA optimizer (Wiest-Daesle et al., 2007)
 - Use of FLAIR as reference sequence

Intensity Inhomogeneity Correction

- IIH is a small spatial variation of intensity in an homogeneous tissue
 - Caused by the imperfection of the magnetic field
- Does not affect “human” radiological assessments
 - But: Reduces performance of many algorithms
- Method applied (Mangin MMBIA 2000)
 - Entropy minimization method
 - No assumptions of MR sequence or number of tissues

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Denoising

- Image additive noise in hardware acquisition
- Method employed
 - (Coupe et al., TMI 2008)
 - Non-Local Means method

	Scanner	T1-w	T2-w	FLAIR
Subject1	3T Siemens	Isotropic 1 mm	3 mm axial slice	3 mm axial slice
Subject2	3T Philips	Isotropic 1 mm	3 mm axial slice	3 mm axial slice
Subject3	3T Siemens	Isotropic 1 mm	Isotropic 1 mm	Isotropic 1 mm

Five different Workflows:

- Basic : No preprocessing before registration.
- NLM : Denoising before registration.
- IIH : Intensity correction before registration.
- IIH+NLM: Intensity correction and then denoising before registration.
- NLM+IIH: Denoising and then intensity correction before registration.

- Preprocessing workflows:
 - With STREMV1, all workflows are tested for the three patients
- STREMV1 vs. STREMV1.5 vs. STREMV2
 - Applying best workflow we compare the different versions of STREMV
- Metrics:
 - DSC with a manually delineated segmentation
 - Execution time

Results

	Subj1	Subj2	Subj3
Basic(v1)	0.31	0.20	0.42
NLM(v1)	0.33	0.29	0.42
IIH(v1)	0.31	0.49	0.53
IIH+NLM(v1)	0.30	0.46	0.48
NLM+IIH(v1)	0.31	0.49	0.56
NLM+IIH(v1.5)	0.31	0.49	0.56
NLM+IIH(v2)	0.38	0.66	0.64

	IIH	NLM	Reg.	Atl.	STREM	Total
Basic(v1)	0	0	339	99	2741	3179
NLM(v1)	0	429	347	136	2486	3398
IIH(v1)	68	0	387	186	1082	1723
IIH+NLM(v1)	68	424	355	48	911	1806
NLM+IIH(v1)	80	429	362	140	923	1934
NLM+IIH(v1.5)	80	429	362	0	584	1455
NLM+IIH(v2)	80	429	362	0	588	1459

- Left: DSC of different subjects and workflows
- Right: Processing time for subject 2

	Subj1	Subj2	Subj3		IIH	NLM	Reg.	Atl.	STREM	Total
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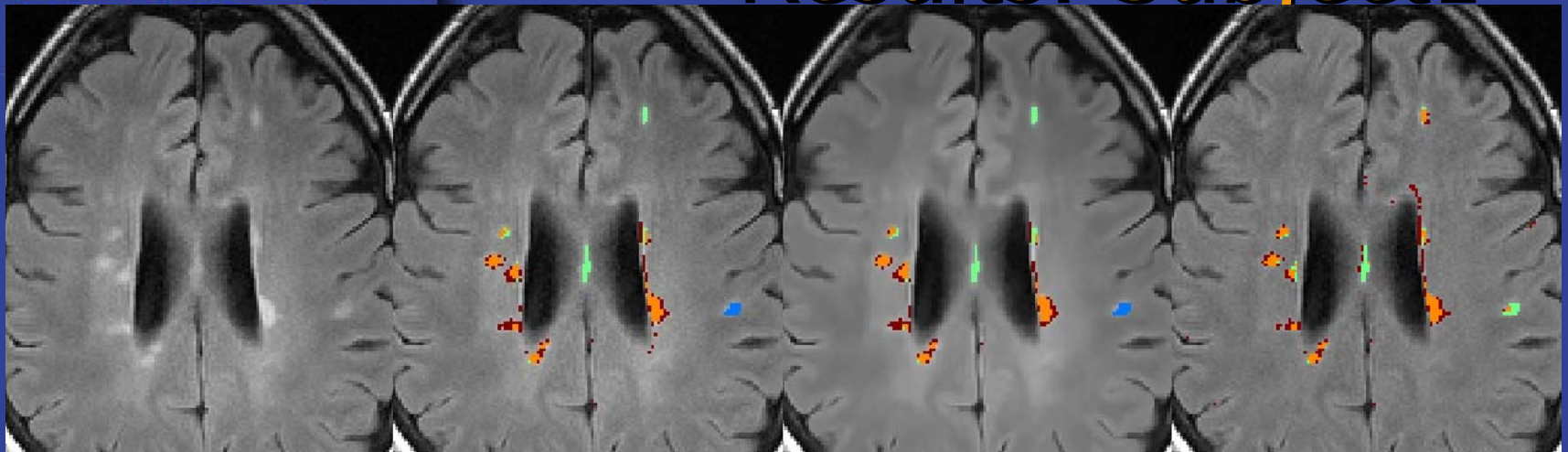
- Performing IIH is more important than denoising
- Sequential association of NLM+IIH better than IIH+NLM

Results

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- New initialization has same solution as atlas based but the workflow is faster
- New rules reduce the number of false positives

Results: Subject1

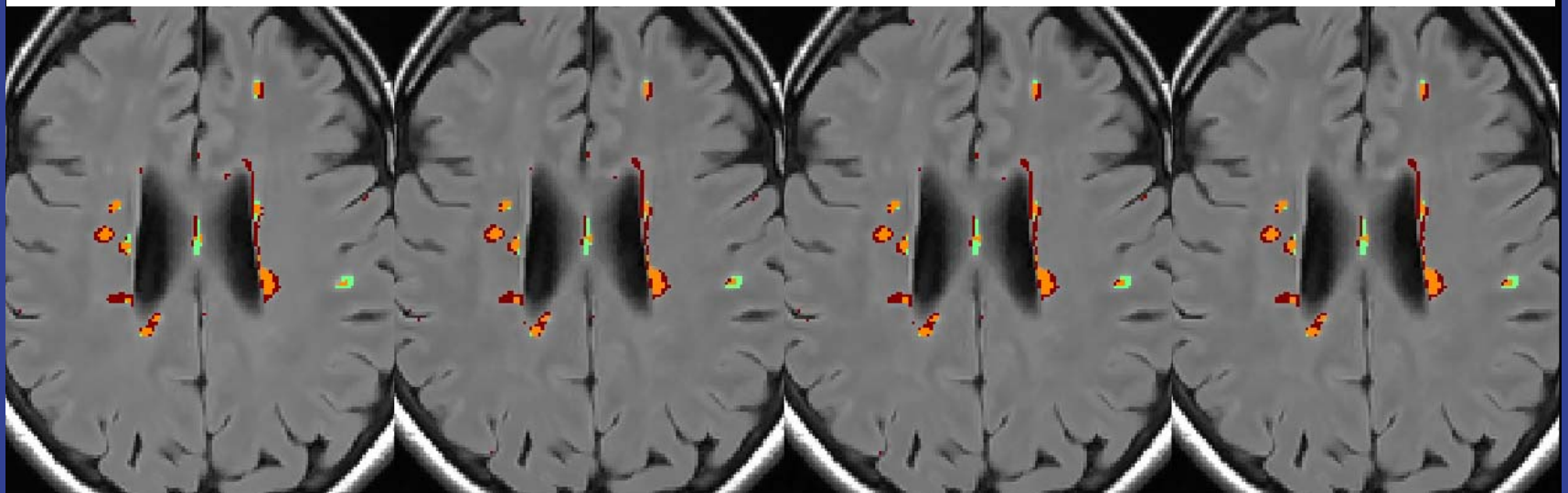


Flair(v1)
IIH+NLM(v1)

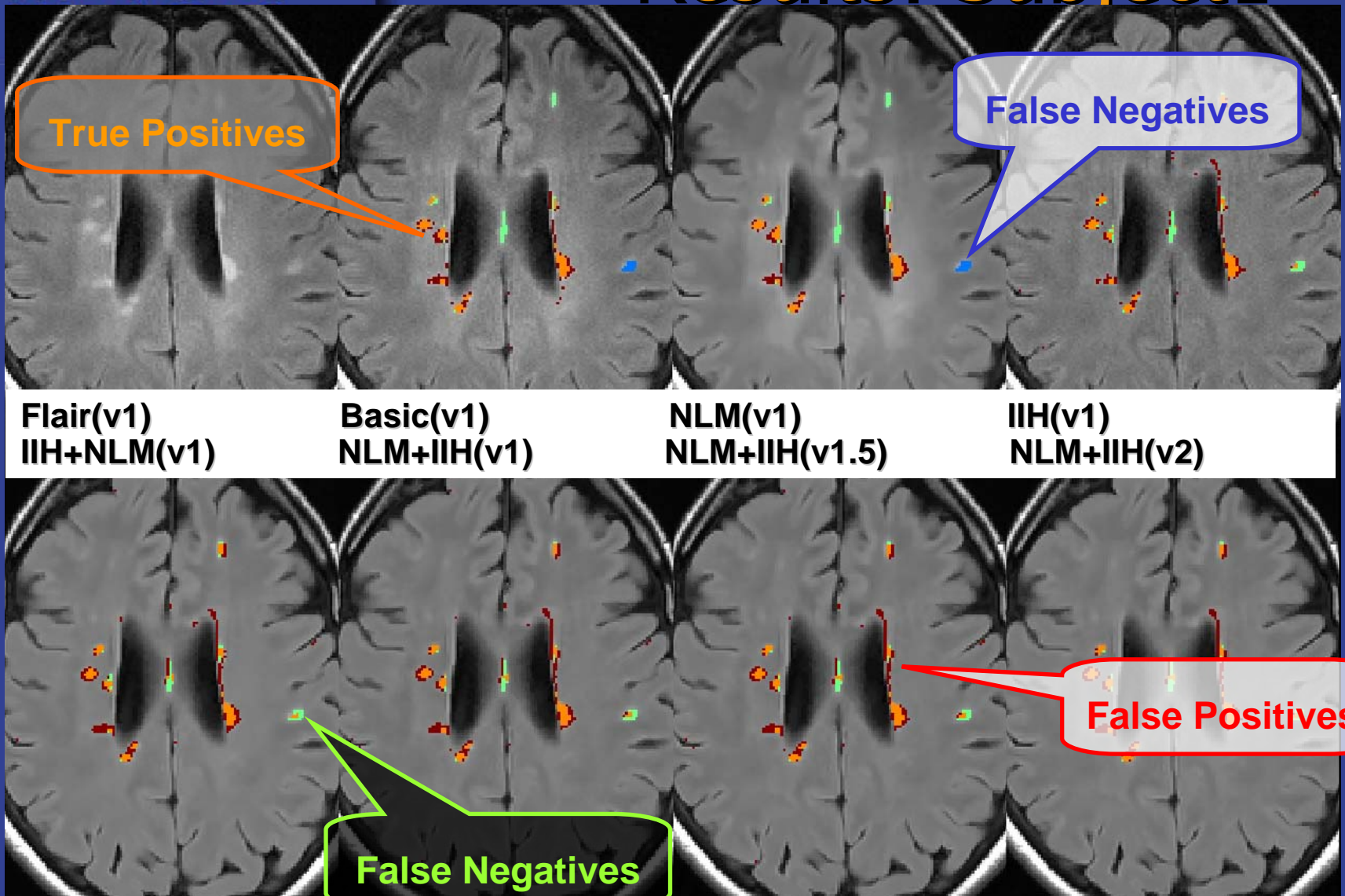
Basic(v1)
NLM+IIH(v1)

NLM(v1)
NLM+IIH(v1.5)

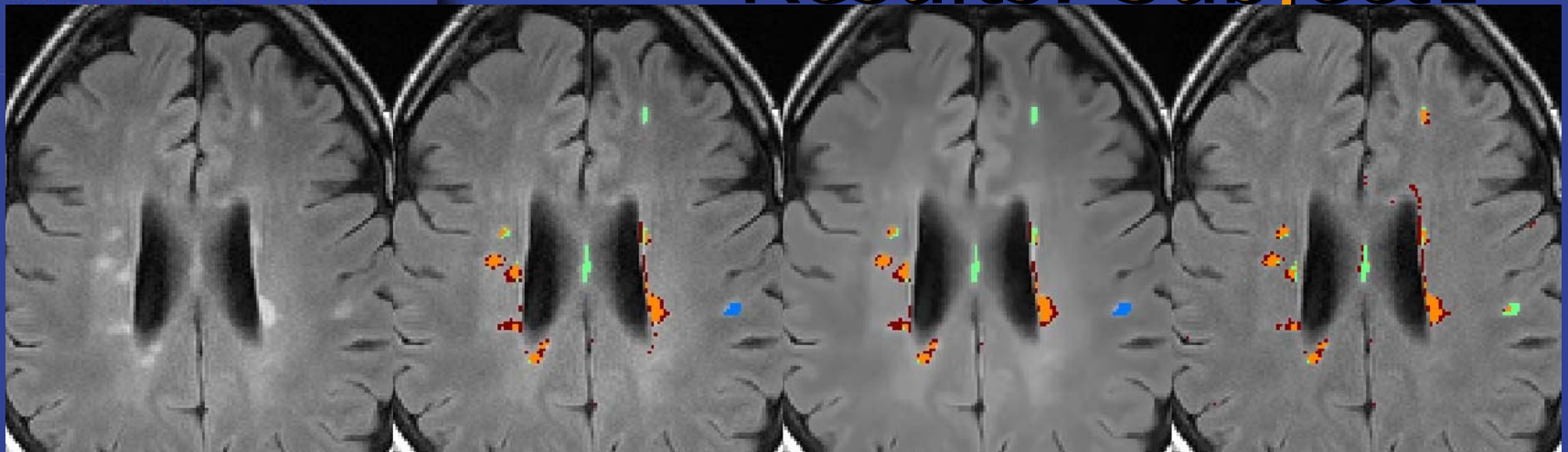
IIH(v1)
NLM+IIH(v2)



Results: Subject1



Results: Subject1

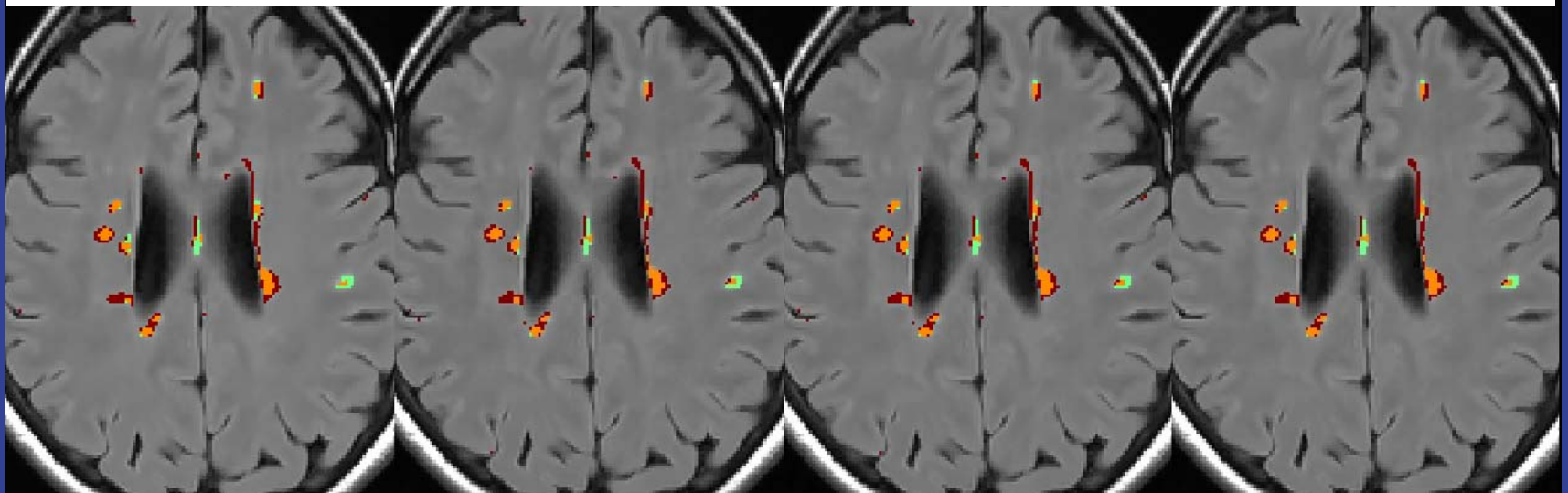


Flair(v1)
IIH+NLM(v1)

Basic(v1)
NLM+IIH(v1)

NLM(v1)
NLM+IIH(v1.5)

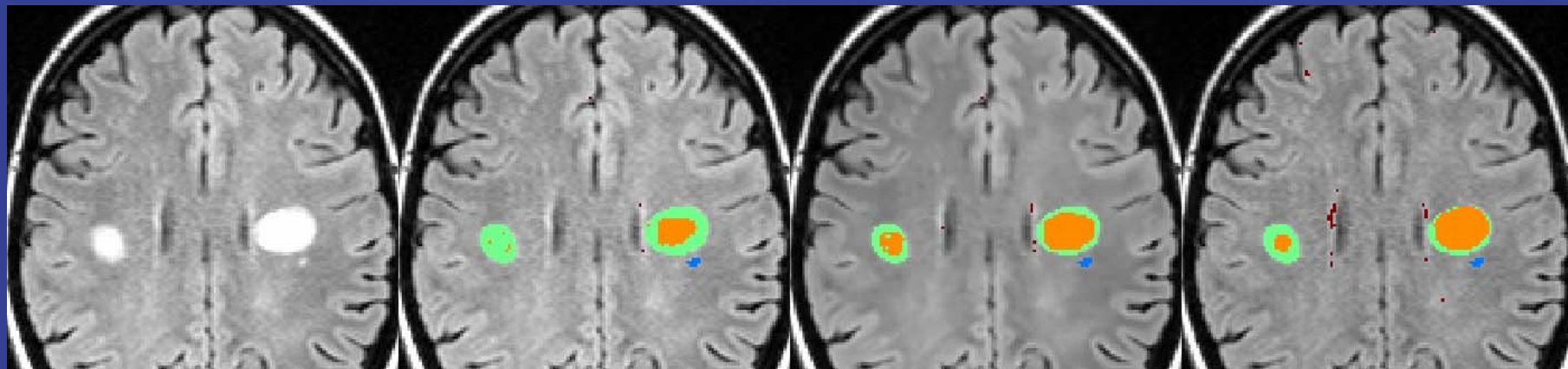
IIH(v1)
NLM+IIH(v2)





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Results: Subject2

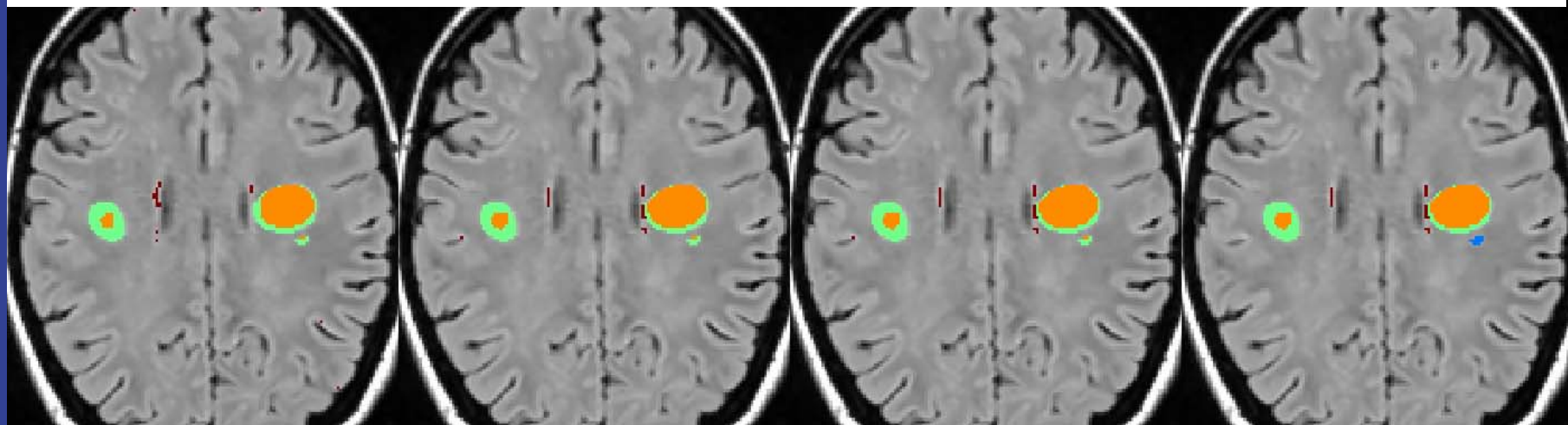


Flair(v1)
IIH+NLM(v1)

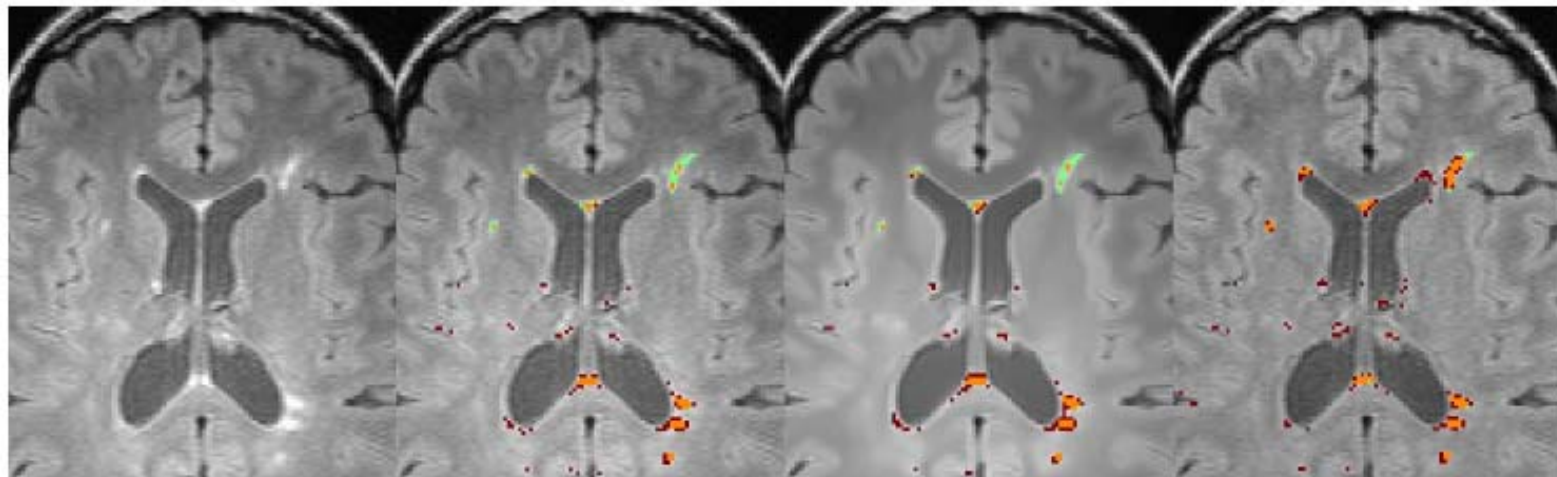
Basic(v1)
NLM+IIH(v1)

NLM(v1)
NLM+IIH(v1.5)

IIH(v1)
NLM+IIH(v2)



Results: Subject3

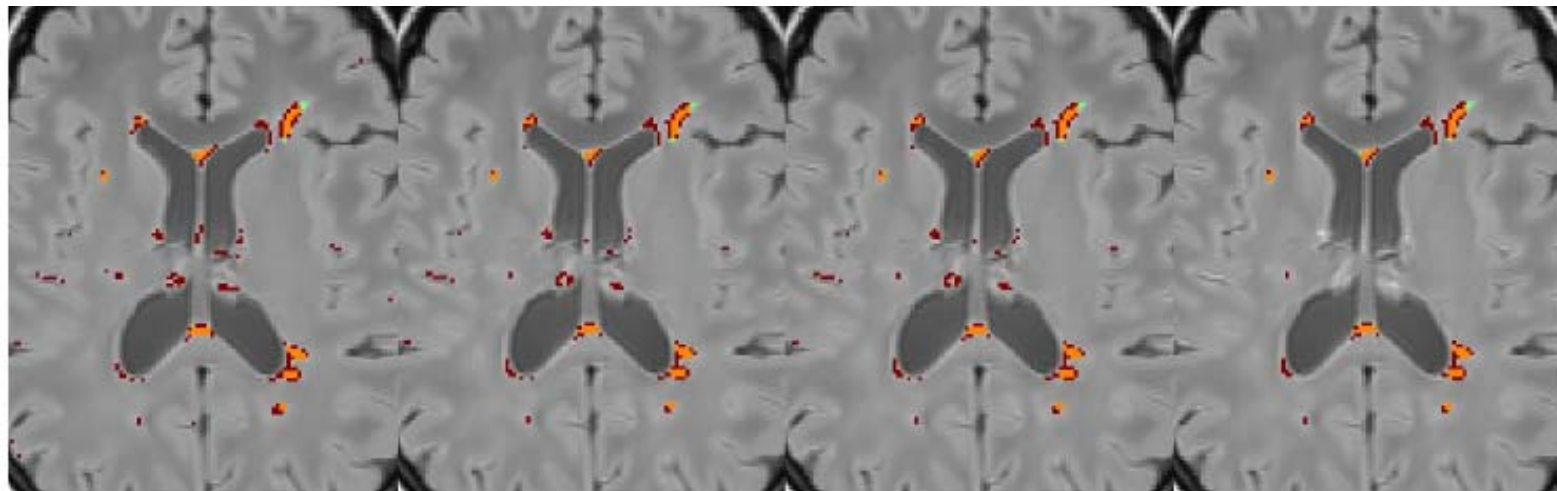


Flair(v1)
IIH+NLM(v1)

Basic(v1)
NLM+IIH(v1)

NLM(v1)
NLM+IIH(v1.5)

IIH(v1)
NLM+IIH(v2)



Conclusions

- Segmentation methods have to be evaluated looking at the whole preprocessing workflow
- We presented our WML and NABT segmentation workflow and showed its impact on the final segmentation result
- Future work:
 - To increase patient number
 - To compare more methods for each preprocessing step

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Thank you very much for
your attention

Supported by Arsep